Design And Evaluation For Anti Hypertensive Management Using Rapimelt Tablet Technology

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Design and Evaluation of Rapimelt Tablet for Anti Hypertensive Management to give quick onset of action by rapidly disintegrating ina few seconds without the need of water with better patient compliance. By performing compatibility studies by IR spectrophotometry, flow properties such as Angle of repose, loose bulk density, Tapped density, % Compressibility, and Hausner's ratio properties. Rapimelt tablets were prepared by direct compression technique using CADMACH 16 station tablet punching machine, equipped with flat round punch of 8.7 mm diameter. Post compression evaluation of prepared Rapimelt tablets were carried out with the help of different pharmacopoeial and non pharmacopoeial (industry specified)tests. Result no interaction was confirmed by IR Spectroscopy. The shape and colour of all the formulations were found to be circular and white in colour and showed good flow properties. The thickness was found to be uniform in specific formulations. Oral rapimelt tablets were formulated by direct compression method and suitable analytical method based on UV-Visible spectrophotometer was developed for the model drug, standard calibration curve prepared to determine the drug content in the prepared tablets and UV analysis was performed to determine the drug during in vitro release studies. The hardness and friability are also within the permitted limits. Formulation TF3 In-vitro Dissolution studies 10 minutes almost total amount of the drug is released 6% crosspovidone (i.e. 96.96%). In such cases, bioavailability of drug is significantly greater and adverse effect is reduced than those observed from conventional tablet dosage form

Keywords: Rapimelt tablets, Hypertensive Management, Crosscarmellose sodium, Treprostinil Diolamine, Drug release kinetics.

INTRODUCTION

Rapimelt tablets oral drug delivery is currently the gold standard in the pharmaceutical industry where it is regarded as the safest, most convenient and most economical method of drug delivery having the highest patient compliance. Methods to improve patient's compliance have always attracted scientists towards the development of fancy oral drug delivery systems.

Among them, Rapimelt tablets drug delivery systems (RmDDS) have acquired an important position in the market by overcoming previously encountered administration problems and contributing to extension of patent life. (RmDDS) have the unique property of rapidly disintegrating and/or dissolving and releasing the drug as soon as they come in contact with saliva, thus obviating the requirement of water during administration.

The oral route of drug administration is popular, convenient and widely accepted method of administering the drugs because of ease of administration, accurate dosage, self-medication, pain avoidance and most importantly patient compliance (6). The major foucs of the formulation scientist is to develop formulations for oral application of newly synthesized drugs since they can be self- administered by the patient. The characteristics of drug, the application desired and the need for any special effects than dictates the type of oral dosage form to be developed (Roy, 1990). The monophasic liquids such as syrups, solutions, elixirs, biphasic liquids such as suspensions, emulsion etc. and solid dosage forms like tablets and capsules and liquid filled capsules are the common types of oral formulations(7).

Hypertension is an important public-health challenge worldwide. In the Lancet literature was published from Jan 1, 1980, to Dec 31, 2002. The studies reported were sex-specific and agespecific prevalence of hypertension in representative population samples. All data were obtained with a standardized protocol and data-collection form(8). Overall, 26.4% (95% CI 26.0-26.8%) of the adult population in 2000 had hypertension (26.6% of men [26.0-27.2%] and 26·1% of women [25·5–26·6%]), and 29·2% (28·8–29·7%) were projected to have this condition by 2025 (29.0% of men [28.6–29.4%] and 29.5% of women [29.1–29.9%]). The estimated total number of adults with hypertension in 2000 was 972 million (957–987 million); 333 million (329–336 million) in economically developed countries and 639 million (625–654 million) in economically developing countries(10). The number of adults with hypertension in 2025 was predicted to increase by about 60% to a total of 1.56 billion (1.54–1.58 billion). Authentic data is needed about the prevalence of hypertension so that corrective measures are taken to prevent and control the disease(19) Under different circumstances an individual's blood pressure levels change but if it is consistently higher under same situations, the person is at risk of developing hypertension. But one blood pressure reading may not be enough to diagnose hypertension; at least two measurements with accuracy are needed to diagnose it. This disease has lifelong implications on person's life(10).

Hypertension (HTN) is considered one of the leading causes of increased cardiovascular disease. Lowering blood pressure does reduce cardiovascular risks; maintaining systolic blood pressure of less than 130 mm Hg demonstrably prevents complications in patients with heart failure, diabetes, coronary artery disease, stroke, and other cardiovascular diseases (11, 12). This activity discusses the guidelines for selecting the appropriate antihypertensive medications. It presents the different classes for first, second and third-line treatments for hypertension and highlights the indications and side effects. It highlights the studies done to compare different classes of antihypertensive medications and indications for each class.

MATERIAL AND METHOD

API and excipients used analytical grade like Crosspovidone, Crosscarmellose Sodium, SSG, MCC102, Aspartame, Mannitol, Magnesium stearate, Talc from Research-Lab Fine Chem Industries, Mumbai, and Loba Chemic Pvt Ltd, Mumbai.

Preparation of Stock solution with Distilled water

100mg of the drug was accurately weighed and transferred into the 100 ml volumetric flask. It was dissolved in sufficient quantity of methanol and volume was made up to the mark with methanol to get a 1000 μ g/ml solution (13). This was the standard stock solution containing 1 mg/ml of model drug (Stock 1).

UV Absorption Maxima (λmax) of drug sample in water

One ml of the above solution was then further diluted to 100 ml with water to get a stock solution of 10 (µg/ml). UV scanning was done for 10 µg/ml drug solution from 200-400 nm using methanol as a blank in schimadzu, UV 1800 spectrophotometer. The wavelength maximum was found to be at 250 nm.

Preparation of the calibration curve

From the stock solution 2, 4, 6, 8, 10 and 12 ml were transferred to 10 ml volumetric flasks and were diluted with the water, up to the mark to obtain concentration of 2, 4, 6, 8, 10 and $12\mu g/ml$ respectively. Absorbance of each solution was measured at 226 nm.

The Standard curve preparation was performed in triplicate. The absorbance was plotted against the concentrations and the graph with the straight line equation and r2 value were obtained (14).

Preparation of Stock solution with 6.8 pH Phosphate Buffer

100mg of the drug was accurately weighed and transferred into the 100 ml volumetric flask. It was dissolved in sufficient quantity of phosphate buffer and volume was made up to the mark with methanol to get a 1000 μ g/ml solution(15). This was the standard stock solution containing 1 mg/ml of model drug. (Stock 1).

UV Absorption Maxima (λmax) of drug sample in 6.8 pH Phosphate Buffer

One ml of the above solution was then further diluted to 100 ml with phosphate buffer to get a stock solution of $10 \, (\mu g/ml)$. UV scanning was done for $10 \, \mu g/ml$ drug solution from 200- $400 \, nm$ using methanol as a blank in schimadzu UV $1800 \, spectrophotometer$. The wavelength maximum was found to be at $250 \, nm$.

Preparation of the calibration curve

From the stock solution 2, 4, 6, 8, 10 and 12 ml were transferred to 10 ml volumetric flasks and were diluted with the phosphate buffer, up to the mark to obtain concentration of 2, 4, 6, 8, 10 and 12µg/ml respectively. Absorbance of each solution was measured at 250 nm(19). The Standard curve preparation was performed in triplicate. The absorbance was plotted against the concentrations and the graph with the straight line equation and r2 value were obtained.

PREFORMULATION PARAMETERS

Pre-formulation testing is defined as investigation of physical and chemical properties of a drug substance alone and when combined with excipients(20). It gives information needed to define the nature of the drug substance and provide frame work for the drug combination with pharmaceutical excipients in the dosage form.

Bulk Density:

Apparent bulk density was determined by pouring presieved drug excipient blend into a graduated cylinder and measuring the volume and weight "as it is". It is represent in gm/mL and is given by

D b = M/V0 Where, M=mass of powder, V0=Bulk volume of the powder

Tapped Density:

It was determined by placing a graduated cylinder, containing a known mass of drug excipient blend, on mechanical tapping apparatus(21). Take the powder to constant volume. The tapped volume was measured by tapping. It expressed in gm/mLand is given by

Dt = M / Vt

Where, M is the mass of powder,

Vt is the tapped volume of the powder.

Carr's index:

It is expressed in percentage and is expressed by

Carr's Index = (ptapped-pbulk) /ptapped*100

With ρ tapped: the tapped bulk density of the material (kg/m3) ρ bulk: the loose bulk density of the material (kg/m3)

Hausner's ratio:

Hausner ratio is an indirect index of ease of powder flow. It is calculated by the following formula.

H = Dt / Db

Where, Dt is the tapped density of the powder Db is the bulk density of the powder. Lower hausner ratio (< 1.25) indicate better flow properties than higher ones (> 1.25).

Angle of Repose:

The frictional forces of a loose powder can be measured by using angle of repose. It is an indicative of the flow properties of the powder. It is defined as maximum angle possible between the surface of the pile of powder and the horizontal plane.

 $\tan (\theta) = h / r \theta = \tan -1 (h / r)$

Where,

 θ is the angle of repose., h is the height in cms,, r is the radius in cms.

The powder mixture was allowed to flow through the funnel fixed to a stand at definite height (h). Angle of repose was calculated by measuring the tallness and radius of the heap of powder formed. Care was taken to see that the powder particles slip and roll over each other through the sides of the funnel. Relationship between angle of repose and powder flow property(22).

FORMULATION DEVELOPMENT

Rapimelt tablets containing 30 mg of model drug were prepared with a total tablet weight of 200 mg. Considering the preformulation studies and the literature survey conducted the excipients were selected and an attempt to produce Rapimelt tablets with ideal mouth feel maintaining the basic tablet properties was made(23).

Selection of Superdisintegrants:

Short disintegration time with good dispersability is the most important characteristics of a rapimelt or mouth dispersible tablets. The necessity of a rapimelt tablet is to disintegrate within

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seconds, in limited amount of the water available in the form of saliva. Different superdisintegrants croscarmellose sodium, crosspovidone, Sodium starch glycol late in the concentration range of 1.5% to 6%were used which act as disintegrates used at various concentrations and a comparative study was carried out.

Selection of diluents

Since direct compression method was followed the choice of directly compressible diluents was important. Microcrystalline cellulose was selected as the filler or diluents owing to its multiple functionality as binder(24), disintegrants compressibility and flow ability. of the various grades available the granular form Avicel PH102 was selected as it had been already reported to provide lower crushing strengths and shorter disintegration times.

Mannitol was selected to produce a cooling and pleasant mouth feel, it was reported that mannitol above the concentration of 33% gives good mouth feel, thus mannitol in all the batches was fixed at a concentration of 40-47%. Besides mannitol also possesses sweetening properties and reduces the gritty mouth feel effect due to microcrystalline cellulose. It also has good compressibility properties and solubility in water.

Selection of additional ingredients

The flow property of the pure drug was found to be moderate (Hauser's ratio \sim 1.4) thus to still improve the flow of the blend magnesium stearate (2.5% to 4%) aslubricant were incorporated also magnesium stearate decreases the hardness of tablets without affecting the disintegration time. Aspartame was used in the concentration of 2.5% to 6% as the sweetener (25).

Rapimelt tablets of model drug was formulated using mannitol, Avicel pH 102 (microcrystalline cellulose) as diluents. Rapimelt tablet was prepared by direct compression technique as it's a cost effective method. Superdisintegrants usedare Crosspovidone, Crosscarmellose sodium, Sodium starch glycol late, disintegrantsodium CMC. Aspartame as sweetening agent. Magnesium stearate (3% to 4%) as lubricant.

Formulation of different batches

The main aim of the present study was to formulate different batches using three various superdisintegrants and other ingredients in varying concentrations. So different batches of formulations was planned accordingly. According to that TF1, TF2, TF3 (with Crosspovidone 1.5%, 3%, 6%), TF4, TF5, TF6 (with Crosscarmellose 1.5%, 3%, 6%) and TF7, TF8, TF9 (with Sodium starch glycollate 1.5%, 3%, 6%). The slight bitter taste of the drug was masked using aspartame (2.5%to 6%) as the sweetening agent (26).

Method of formulation

Direct compression method.

The model drug (NMD) is thoroughly mixed with the superdisintegrants, and then other excipients are added to the mixer and passed through the sieve (#:40). Collect the powder mixer, blend with magnesium stearate (pre sieved), and subject the blend for tablet compression(27).

Representation of DirectCompression Technique for design of RapimeltTablets

The drug and the excipients were passed through sieve no: 40 except lubricant. The blend was further lubricated with Magnesium stearate (#:60)and the powder blend is subjected to drying for removal of moisture content and was compressed by direct compression method by using

flat faced punches in CADMACH 16 punches tablet punching machine. Round punches measuring 8.7mm diameter were used for compression(28). Tablet of 200mg was prepared by adjusting hardness and volume screw of compression machine properly

Table 1: Formulations of different batches

Inquadiants(mg)		Formulation Code									
Ingredients(mg)	TF1	TF2	TF3	TF4	TF5	TF6	TF7	TF8	TF9		
Treprostinil Diolamine	30	30	30	30	30	30	30	30	30		
Crosspovidone		6	12	-	-	-	-	-	-		
Crosscarmellose sodium	-	-	-	3	6	12	-		-		
SSG	-	-	-	-	-	-	3	6	12		
MCC102	66	64	58	66	64	58	66	64	58		
Aspartame	10	10	10	10	10	10	10	10	10		
Mannitol	80	80	80	80	80	80	80	80	80		
Magnesium stearate	6	6	6	6	6	6	6	6	6		
Talc	4	4	4	4	4	4	4	4	4		

Evaluation of tablets Hardness test(29):

Using a Monsanto hardness tester the rigidity (hardness) of the tablet was determined

Friability:

The friability of a sample of 20 tablets was measured using a Roche friabilator (Electrolab). 20 previously weighed tablets were rotated at 25 rpm for 4 min. The weight loss of the tablets before and after

Measurement was calculated using the following formula

Percentage friability=Initial weight –Final weight x100

Initial weight

Weight Variation:

It was performed as per the method given in the united state pharmacopoeia. Twenty tablets were selected randomly from each formulation, weighed individually and the average weight and %variation of weight was calculated.

Tablet thickness:

Tablet thickness is an important characteristic in reproducing appearance and also in counting by using filling equipment. Some filling equipment utilizes the identical thickness of the tablets as a counting mechanism. Ten tablets were taken and their thickness was recorded Vernier calipers using micrometer.

Drug Content Uniformity:

Selected twenty tablets randomly and powdered. A quantity of this powder corresponding to 200mg of model drug was dissolved in 100 ml of 6.8pH phosphate buffer, stirred for 15 min and filtered. The 1ml of filtrate was diluted with 100 ml with 6.8pH phosphate buffer. Absorbance of this solution was measured at 250nm using 6.8 pH phosphate buffer as blank

and content of drug was estimated 16.

In-vitro Disintegration Time:

Disintegration times for rapimelt tablets were determined using USP tabletdisintegrationapparatus with saline phosphate buffer of pH6.8 as medium. Maintained the medium tempat 37±2°. The time in minute taken for complete disintegration of the tablets with no palatable mass remaining in the apparatus was measured.

Wetting Time:

A piece of tissue paper folded twice was placed in a small Petri dish (ID = 6.5cm) containing 6 mL of simulated saliva pH, a tablet was put on the amaranth powder containing paper the time required for upper surface of the tablet for formation of pink color was measured.

Water absorption ratio:

For measuring water absorption ratio, the weight of the tablet before keeping in the petri dish is noted (W_b) . The wetted form of tablet was taken from petridish and reweighed (W_a) . The water absorption ratio (R) can be the determined according to the following equation.

 $R=100 \text{ x } (W_a-W_b) / W_b$

In-vitro dispersion time:

In vitro dispersion time was measured by dropping a tablet in a measuring cylinder containing 6ml of pH6.8 (simulated saliva fluid). Tablets from each formulation werer and omly selected and in vitro dispersion time is expressed in seconds.

In-vitro Dissolution studies(30):

Dissolution of the tablet of each batch was carried out using USPXXIII dissolution type II apparatus (ELECTRO LAB) using paddles at 50 rpm. As per the official recommendation of IP 900ml of 6.8 pH of phosphate buffer used as dissolution medium—and the temperature of the medium was set at 37 ± 0.5 0C. 5 ml of sample was withdrawn at predetermined time interval of 2 .,4., 6., 8 and 10 min. And same volume of fresh medium was replaced. The withdrawn samples were analyzed by an UV spectrophotometer at 250 nm using buffer solution as blank solution.

Drug release kinetics:

As a model independent approach, comparison of time taken for the given proportion of the active drug to be dissolved in the dissolution medium and figures such as T_{50} and T_{90} were calculated by taking the time points of 50% and 90% of the drug dissolved and another parameter dissolution efficiency (DE) suggested by Khan were employed. DE is defined as the area under the dissolution curve up to the time t expressed as a percentage of the area of the rectangle described by 100% dissolution in the same time(31).

where t is the time, y is the percentage of drug dissolved at time t, and $\int_0^t yxdt$ is the area under the curve.

Zero order kinetics:

The zero order release has the ability to deliver a drug at a rate independent of time and drug

concentration in a dosage form. Zero order ensures a steady amount of drug is released over time(32). This model represents the drug dissolution from dosage forms that do not disaggregate and release the drug slowly including transdermal systems or matrix tablets with low soluble drugs. The model is represented by the Equation below

Q1 = Q0 + K0t

Where (Q1) is the amount of drug dissolved;

(t) is the time;

(Q0) is the initial amount of drug in the solution; and

(K0) is the zero order release constant.

First order kinetics:

This first order model is used to describe the absorption and elimination of some drugs. This model releases the drug proportionally to the amount of drug remaining in the interior of the dosage form, allowing for the amount of drug released per unit of time to diminish. The dosage forms which follow this dissolution profile include water soluble drugs in porous matrices. The model is represented by Equation 9.2 below(33).

logQ1 = logQ0 + K1t2.303

Where (Q1) is the amount of drug released; (Q0) is the initial amount of drug in solution; (t) is the time; and (K1) is the first order release constant.

Hixon-crowellcubth root model:

The Higuchi model is used to study the release of water soluble and low soluble drugs incorporated in a semi-solid or solid matrix. This model describes drug release as a diffusion process based on Fick's law. The Higuchi model is used to describe drug dissolution from several types of modified release dosage forms such as transdermal systems or matrix tablets containing water soluble drugs. The model is represented by Equation 9.3 below(34).

 $Q1=KH\sqrt{t}$

Where (Q1) is the amount of drug released; (KH) is the Higuchi dissolution constant; and (t) is the time.

Higuchi model:

The Higuchi model is used to study the release of water soluble and low soluble drugs incorporated in a semi-solid or solid matrix. This model describes drug release as a diffusion process based on Fick's law. The Higuchi model is used to describe drug dissolution from several types of modified release dosage forms such as transdermal systems or matrix tablets containing water soluble drugs. The model is represented by Equation below .

 $O1=KH\sqrt{t}$

Where (Q1) is the amount of drug released (KH) is the Higuchi dissolution constant; and (t) is the time.

Korsmeyer-peppas model:

The Korsmeyer-Peppas model is a simple model relating, exponentially, the drug release to the elapsed time. The different release mechanisms are characterized by using an n-value, which differs depending on a slab or a cylinder(35). This model is used to analyze polymeric dosage forms that do not have a well-known release mechanism or more than one type of release is occurring simultaneously. The model is represented by Equation $F=MtM\infty /=Kmtn$

Where (F) is the fraction of drug release at specific time; (Mt) is the amount of drug release; $(M\infty)$ is the total amount of drug in dosage form; (Km) is the structural and geometric constant; and (n) is the release exponent.

Table 2: Effect of 'n' v	alue on drug trans	sport mechanism
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Release exponent(n)	Drug transport mechanism
n=0.5	Fickian diffusion
0.5 <n<1< td=""><td>Non-fickian diffusion</td></n<1<>	Non-fickian diffusion
n=1	Case II transport
n>1	Super case II transport

Stability Studies:

The purpose of stability testing is to provide evidence on how the quality of a drug substance or drug product varies with time under the influence of a variety of environmental factors such as temperature, humidity and light, enabling recommended storage conditions, retest periods and shelf life(36). Generally, the observation of the rate at which the product degrades under normal room temperature requires a long time. To avoid this undesirable delay, the principles of accelerated stability studies are adopted.

ICH specifies the length of study and storage conditions.

Long-Term Testing: 25^0 C $\pm 2^0$ C/ 60 % RH ± 5 % for 12 Months **Accelerated Testing:** 40^0 C $\pm 2^0$ C/75% RH ± 5 % for 6 Months

Stability studies were carried out at 40^{0} C \pm 2^{0} C/75% RH \pm 5% for all the formulations for a period of 3 months.

The selected formulations were closely packed in aluminium foils and then stored at 40° C \pm 2° C/75% RH \pm 5% in stability chamber for 3 months and evaluated for their physical appearance, drug content and in-vitro drug release studies at intervals of 1month. The shelf life period of the prepared buccal tablets is determined by using similarity factor(37).

RESULTS AND DISCUSSION

Objective of this study was to formulate directly compressible orally disintegrating tablets of Treprostinil Diolamine with sufficient mechanical integrity, content uniformity, and acceptable palatability to assist patients of any age group for easy administration for the treatment of Hypertension (Pulmonary Arterial Hypertension), nausea and vomiting, and motion sickness for rapid dissolution and absorption of drug which may produce rapid onset of action. It is also helpful for vestibular symptoms of other origins.

Treprostinil is a vasodilator that is used for the treatment of pulmonary arterial hypertension. Treprostinil is a chemically stable prostacyclin analog. Its principal pharmacologic action is direct vasodilation, which causes reduction of pulmonary and systemic arterial pressure, reducing right and left ventricular afterload; therefore improves the cardiac output. It also has an antiplatelet effect(38).

Preformulation Studies

General properties

Description : White to cream color crystalline powder.

Solubility Profile : Solubility in different pH buffers and solvents is given below.

Table 3: Solubility in different pH buffers is given below

pH Buffers	Solubility (mg/mL)	Solubility
1.2	Not soluble	Practically insoluble
2.4	Not soluble	Practically insoluble
4.5	Not soluble	Practically insoluble
6.8	100.34	Freely soluble
7.5	101.04	Freely soluble

Table 4: Solubility in different Solvent is given below

Name of the Solvent	Solubility
Methanol	Freely soluble
Ethanol	Freely soluble

N,N- Dimethyl formamide	Freely soluble
Water	Freely soluble

Melting Point by DSC: About 109°C.

Melting point by DSC has been performed for three production scale batches of Treprostinil Diolamine and the results are depicted below;

Table 5: Melting Point by DSC

Batch#	Results
TD01	109.37°C
TD02	109.31°C
TD03	109.57°C

Hygroscopicity:: Slightly Hygroscopic.

Calibration curve of Treprostinil Diolamine

Preparation of Stock solution with Distilled water

100mg of the drug was accurately weighed and transferred into the 100 ml volumetric flask. It was dissolved in sufficient quantity of methanol and volume was made up to the mark with methanol to get a 1000 μ g/ml solution. This was the standard stock solution containing 1 mg/ml of model drug (Stock 1).

UV Absorption Maxima (λmax) of drug sample in water

One ml of the above solution was then further diluted to 100 ml with water to get a stock solution of 10 (μ g/ml). UV scanning was done for 10 μ g/ml drug solution from 200-400 nm using methanol as a blank in schimadzu UV 1800 spectrophotometer. The wavelength maximum was found to be at 250 nm.

Preparation of the calibration curve

From the stock solution 2, 4, 6, 8, 10 and 12 ml were transferred to 10 ml volumetric flasks and were diluted with the water, up to the mark to obtain concentration of 2, 4, 6, 8, 10 and 12µg/ml respectively. Absorbance of each solution was measured at 226 nm.

The Standard curve preparation was performed in triplicate. The absorbance was plotted against the concentrations and the graph with the straight line equation and r2 value were obtained(39).

Preparation of Stock solution with 6.8 pH Phosphate Buffer

100mg of the drug was accurately weighed and transferred into the 100 ml volumetric flask. It was dissolved in sufficient quantity of phosphate buffer and volume was made up to the mark with methanol to get a 1000 μ g/ml solution. This was the standard stock solution containing 1 mg/ml of model drug (Stock 1).

UV Absorption Maxima (λmax) of drug sample in 6.8 pH Phosphate Buffer

One ml of the above solution was then further diluted to 100 ml with phosphate buffer to get a stock solution of 10 (µg/ml). UV scanning was done for 10 µg/ml drug solution from 200-400 nm using methanol as a blank in schimadzu, UV 1800 spectrophotometer. The wavelength maximum was found to be at 250 nm.

Preparation of the calibration curve

From the stock solution 2, 4, 6, 8, 10 and 12 ml were transferred to 10 ml volumetric flasks and were diluted with the phosphate buffer, up to the mark to obtain concentration of 2, 4, 6, 8, 10 and $12\mu g/ml$ respectively. Absorbance of each solution was measured at 250 nm. The Standard curve preparation was performed in triplicate(40). The absorbance was plotted against the concentrations and the graph with the straight line equation and r^2 value were obtained.

Table 6: Standard Calibration curve of Treprostinil Diolamine with Distilled water

S.No.	Concentration(mcg/ml)	Absorbance
1	0	0
2	2	0.208
3	4	0.435
4	6	0.646
5	8	0.808
6	10	0.996
7	12	1.234

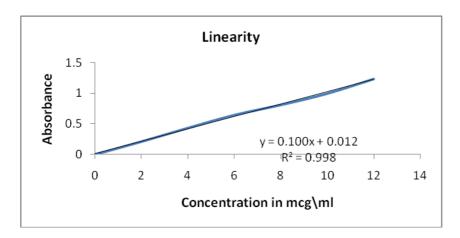


Figure 1: Standard Calibration curve of Treprostinil Diolamine with Distilledwater In the current investigation, analytical method obeyed beer-lamberts law in the concentration range of $2\text{-}12\mu\text{g}$ /ml and it was suitable for the estimation of Treprostinil Diolamine using Distilled water. The value of correlation coefficient(r) for the linear regression equation was found to be more than 0.99 which indicates a positive correlation between the concentration of drug and corresponding absorbance values.

Table 7: Standard Calibration curve of Treprostinil Diolamine with 6.8pH phosphate buffer

S.No.	Concentration(mcg/ml)	Absorbance
1	0	0
2	2	0.208
3	4	0.397
4	6	0.657
5	8	0.846
6	10	1.045
7	12	1.234

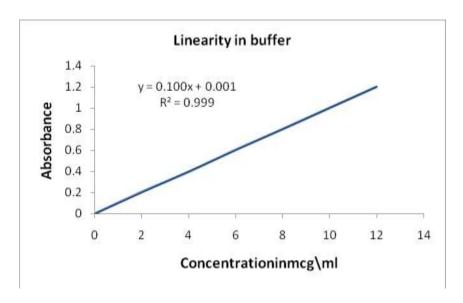


Figure 2: Standard Calibration curve of NMD with 6.8pH phosphate buffer

In the current investigation, analytical method obeyed beer-lamberts law in the concentration range of 2-12 μ g/ml and it was suitable for the estimation of Treprostinil Diolamine using phosphate buffer of pH 6.8. The value of correlation coefficient (r) for the line arregression equation was found to be more than 0.99 which indicates positive correlation between the concentration of drug and corresponding absorbance values(41).

FT-IR studies

Table 8: FT-IR inter pretations of pure drug and physical mixtures

				Observed peaks						
S. No	runctional	Charact eristic peaks	Trepro stinil Diola mine	Trepro stinil Diola mine: MCC	Trepro stinil Diola mine: SSG	repro		Treprostinil	Treprostinil Diolamine:M g.stearate	
1	C-H (Aromatic bending)	680- 862cm ⁻¹	782.18 cm ⁻¹	782.18 cm ⁻¹	781.30 cm ⁻¹	781.20 cm ⁻¹	782.18c m ⁻¹	783.12cm ⁻¹	782.13cm ⁻¹	
2	NO ₂ (stretching)	1300- 1600cm ⁻	1369.5 4cm ⁻¹	1368.5 6cm ⁻¹	1369.5 3cm ⁻¹	1369.5 3cm ⁻¹	1369.52 3cm ⁻¹	1369.523cm -1	1369.53cm-1	
3	C=C (Aromaticst retching)	1400- 1600cm ⁻	1465.9 7cm ⁻¹		1415.8 2cm ⁻¹			1415.82cm- 1	1426.43cm ⁻¹	

4	N-H (bending)	1580- 1650cm ⁻	1626.0 6cm ⁻¹	1627.0 2cm ⁻¹	1638.6 8cm ⁻¹	1637.6 4cm ⁻¹	1627.98 cm ⁻¹	1626.07cm- 1	1624.14cm-1
5	C-H (stretching)	2850- 3000cm ⁻	2973.4 2cm ⁻¹	2936.7 4cm ⁻¹	2937.7 2cm ⁻¹	2936.7 4cm ⁻¹	2938.67 cm ⁻¹	2943.52cm- 1	2934.83cm-1
6	O-H (stretching)	3200- 3500cm ⁻	3411.2 7cm ⁻¹	3258.8 2cm ⁻¹	3397.2 7cm ⁻¹	3272.3 8cm ⁻¹	3273.35 cm ⁻¹	3261.78cm-1	3271.42cm-1

Figure 3: FT-IR spectra of Treprostinil Diolamine



FT-IR spectra of pure Treprostinil Diolamine and the physical mixtures of drug and excipients were given in Table 7.3 and Figure 7.3, 7.4, 7.5,7.6 7.7 and 7.9. Pure Treprostinil Diolamine showed principal absorption peaks at782.17cm⁻¹(C-H aromatic bending), 1368.54cm⁻¹ (NO₂stretching), 1464.94 cm⁻¹(C=C aromatic stretching), 1626.06cm⁻¹ (N-H bending), 2972.38 cm⁻¹ (C-H stretching) and 3411.22cm⁻¹ (O-H stretching). The identical peaks of C-H aromatic bending, NO₂ stretching, C=C aromatic stretching, N-H bending, C-H stretching and O-H stretching, vibrations were also noticed in the spectra of physical mixtures which contains drug and excipients. FT-IR spectra revealed that there was no interaction between the drug and the excipients used for fast dissolving tablets preparation.

Pre-compression parameters Treprostinil Diolamine fast dissolving tablets.

The angle of repose less than 31.82, which reveals good flow property it shown in for formulations TF1–TF9 .The loose bulk density and tapped bulk density for all formulation (TF1 – TF9) varied from 0.442 gm/cm³ to 0.485gm/cm³ and 0.502 gm/cm³to 0.593 gm/cm³ respectively. The results of carr's consolid at e index or % compressibility index for the entire

formulation (TF1 – TF9) blend range from 15 to 19 shows fair flow properties.

Formulations of different batches

The rapimelt tablet of Treprostinil Diolamine will be prepared by direct compression method by adding various polymers and super disintegrants.

Table 9: Formulations of different batches

Ingredients(mg)	Formulation Code									
ingredients(ing)	TF1	TF2	TF3	TF4	TF5	TF6	TF7	TF8	TF9	
Treprostinil Diolamine	20	20	20	20	20	20	20	20	20	
Crosspovidone	3	6	12	-	-	-	-	-	-	
Crosscarmellose sodium	-	-	-	3	6	12	-		-	
SSG	-	-	-	-	-	-	3	6	12	
MCC102	76	74	68	76	74	68	76	74	68	
Aspartame	10	10	10	10	10	10	10	10	10	
Mannitol	80	80	80	80	80	80	80	80	80	
Magnesium stearate	6	6	6	6	6	6	6	6	6	
Talc	4	4	4	4	4	4	4	4	4	

Table 10: Evaluation of tablet blend for formulations (TF1-TF9)

Formulation	Bulk Density (g/cc)	Tapped Density (g/cc)	Hausner's ratio	npressibility index (%)	Angle of repose
TF1	0.463	0.573	1.22	19.2	29.46
TF2	0.422	0.504	1.17	15.6	27.64
TF3	0.457	0.543	1.23	15.7	25.55
TF4	0.468	0.558	1.26	16.5	26.24
TF5	0.486	0.592	1.12	18.23	27.22
TF6	0.462	0.557	1.22	17.3	30.37
TF7	0.476	0.574	1.23	16.7	28.47
TF8	0.452	0.555	1.27	18.8	25.72

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TF9	0.441	0.538	1.28	17.7	31.83

Postcompression parameters Treprostinil Diolamine fast dissolving tablets.

Table 11: Evaluation of Rapimelt tablets for formulations (TF1– TF9)

Formulation	Hardness (kg/cm2)	iability (%)	Weight(mg)	Thickness(mm)	Drug content(%)
TF1	3.0 ± 0.16	0.24	201±0.58	3.9 ± 0.0	97.4
TF2	2.8 ± 0.22	0.22	198±0.62	4.2±0.02	97.7
TF3	3.1±0.17	0.27	201±0.46	3.7 ± 0.07	98.3
TF4	2.9±0.14	0.23	202±0.87	3.8±0.10	97
TF5	3.2 ± 0.17	0.29	204±0.45	3.9 ± 0.03	98.43
TF6	2.8 ± 0.23	0.33	198±0.64	3.9 ± 0.06	100.7
TF7	3.2 ± 0.25	0.27	201±0.78	3.8 ± 0.15	97.2
TF8	2.9 ± 0.22	0.28	201±0.87	3.9 ± 0.03	98.2
TF9	2.8 ± 0.18	0.23	203±0.75	4.1 ± 0.01	95.34

The hardness values ranged from 2.8±0.17 kg/cm²to 3.2±0.25 kg/cm²for formulation (TF1-TF9) and were almost same. The friability values were found to be within the limit (0.5-1%). The above evaluation parameter showed no significant difference between TF1, TF2, TF3, TF4, TF5, TF6, TF7, TF8, TF9 formulations. The entire tablet passes weight variation test as the average % weight variation was within the Pharmacopeia limit of 7.5%. It was found to be 198±0.62 mg to 204±0.55 mg. The weight of all the tablets was found to be uniform with less deviation(42). The maximum concentration among all the formulations was found to be 100.8% and minimum % drug content from all formulation was found to be 95.34%. The results of drug content of all batches are shown in.

Evaluation of Treprostinil Diolamine Rapimelt fast dissolving tablets.

Table 12: Evaluation of Rapimelt fast dissolving tablets for formulations (TF1-TF9)

Formulation	sintegration time (sec)	Wetting time(sec)	Water absorption ratio(%)	In vitro dispersion time(sec)
TF1	8	20	19.42	8
TF2	6	15	22.47	5
TF3	5	12	19.78	5
TF4	10	16	16.13	15
TF5	9	14	17.27	11

TF6	8	19	12.17	9
TF7	18	27	15.32	14
TF8	10	20	12.047	12
TF9	9	20	13.92	8

Disintegration test carried out in modified dissolution apparatus, it shows the formulations with 1.5%, 3%, 6% Sodium Starch Glycolate showed high value for disintegrating time as 18,10, 8 secs. The results showed that the disintegration time of TF1, TF2, TF3 with 1.5%, 3%, 6% CP formulations to be as 8, 6, 5 secs respectively and is almost better than TF4, TF5, TF6, TF7, TF8, TF9 formulations and comparative profile.

Wetting time is closely related to the inner structure of tablet. The experiment mimics the action of saliva in contact with the tablet to illustrate the water uptake and subsequent wetting of tablet. This shows the wetting process was very rapid in almost all formulations. This may be due to the ability of swelling followed by breaking and also capacity of water absorption and causes swelling. It was found to be in the range of 14 secs to 27secs. It shows crosspovidone formulations TF1, TF2, TF3 (1.5 - 6%) have better wetting time comparing with that of croscarmellose sodium starch glycolate, and comparative profile result was shown in table 12.

Water absorption ratio which is important criteria for understanding the capacity of disintegrates to swell in the presence of little amount of water, was calculated. It was found to be in the range of 12.17 to 22.47%. This shows that all the formulations have good water absorption capacity result was shown in table 12.

The in-vitro dispersion time is measured by time taken to uniform dispersion, the rapid dispersion. It was found to be in the range of 5secs to 15secs (Graph). The result showed that the in vitro dispersion time of TF1, TF2, and TF3 formulations is almost equal and better than TF4, TF5, TF6, TF7, TF8, TF9 formulations and comparative profile result was shown in Table 14.

In-vitro dissolution studies of Treprostinil Diolamine Rapimelt fast dissolving tablets.

Table 13: Cumulative % drug release for formulations (TF1–TF9)

Cumulative % drug release									
Time	TF1	F2	TF3	TF4	TF5	TF6	TF7	TF8	TF9
2Min	55.14	58.9	65.5	48.07	51.42	62.7	45.93	50.54	57.98
4Min 68.7 72.1 74.9 57.28 61.54 71.12 55.97 61.72 61.07								61.07	

6Min	71.13	80	82.64	72.92	76.55	81.16	71.44	73.22	77.24
8Min	81.8	87.07	89.06	79.68	84.61	86.57	76.05	81.83	84.12
10Min	91.17	94.83	96.96	88.42	93.32	94.18	85.2	87.07	89.24

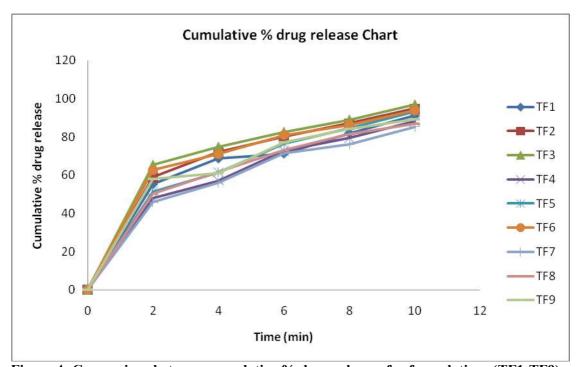


Figure 4: Comparison between cumulative % drug releases for formulations (TF1-TF9)

Dissolution is carried out in USP-2 type apparatus at 50rpm in the volume of 500 ml dissolution media (phosphate buffer pH 6.8) for 10 minutes. At the end of 10 minutes almost total amount of the drug is released (i.e. 96.96%), from the formulation prepared by the direct compression method with 6% crosspovidone result was shown in table 13.

Drug release kinetics of Treprostinil Diolamine fast dissolving tablets.

Correlation coefficient (r) & rate constant (k) Values of Treprostinil Diolamine Rapimelt tablets containing Crospovidone, croscarmellose sodium, sodium starch glycolate.

Table 14: Drug release kinetics

Kinetic model		TF1	TF2	TF3	TF4	TF5	TF6	TF7	TF8	TF9
Zero	r	0.94367	0.9392	0.9179	0.9365	0.9318	0.9155	0.9423	0.8382	0.8978
order	k	17.14	18.26	18.72	14.32	15.37	17.78	13.99	15.42	15.42

	r	0.9943	0.9913	0.9647	0.9942	0.9737	0.9832	0.9954	0.9927	0.9797
Higuchi	k	35.18	37.09	39.08	29.63	31.80	37.17	28.83	31.76	32.72
First	r	0.9962	0.9938	0.9992	0.9981	0.9994	0.9902	0.9989	0.9992	0.9823
order	k	0.2698	0.3192	0.3456	0.2127	0.2466	0.3105	0.2057	0.241	0.24
Dannag	r	0.9796	0.9996	0.9985	0.9893	0.9914	0.9127	0.9913	0.9972	0.9614
Peppas	k	0.293	0.2894	0.2388	0.3878	0.3758	0.2512	0.3894	0.3489	0.28823
Hixson-	r	0.9658	0.9703	0.9627	0.9815	0.9855	0.858	0.9762	0.9742	0.9602
crowell	k	0.3717	0.4023	0.4284	0.2865	0.3162	0.3932	0.2776	0.3177	0.3177
DE10)	44.72	47.47	51.48	38.36	41.13	49.12	36.96	40.47	44.37
DE30)	58.97	63.63	66.89	54.53	57.96	64.55	52.84	56.59	59.72
T50		1.82	1.70	1.53	2.43	1.93	1.58	2.82	1.97	1.72
T90		9.74	8.74	8.23	0	9.27	8.93	0	0	0

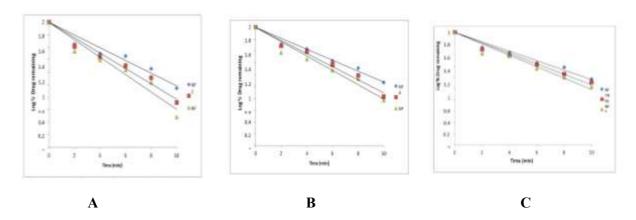


Figure 5: First order plots of Treprostinil Diolamine Rapimelt tablets containing (A) crosspovidone,(B) Croscarmellosesodium, (C) Starch glycolate

The drug release profiles of Treprostinil Diolamine rapimelt tablets were fitted to various kinetic models such as Zero order, First order, Higuchi, Peppas and Hixson-Crowell. The dissolution parameters such as dissolution efficiency (DE) at 10 and 30minutes were increased proportionately. Half-life of drug i.e., T₅₀ was found to be 181,1.70, 1.53, 2.42, 1.94, 1.59, 2.81, 1.98 and 1.73 min for TF1, TF2, TF3, TF4, TF5, TF6, TF7, TF8 and TF9 formulations respectively. Shelf-lifeofthedrugi.e.,T₉₀wasfoundtobe 9.75, 8.75, 8.24, 9.28 and 8.92 minutes for TF1, TF2, TF3, TF5 and TF6 formulations respectively. The drug release data of Treprostinil Diolamine fast dissolving tablets have treated with different kinetic models are

shown in Table 14. The drug release patterns of Treprostinil Diolamine fast dissolving tablets had followed the first order kinetic model. This release patterns are evident with the correlation coefficient 'r' values which are nearer to 1. The first order plots for all Treprostinil Diolamine fast dissolving tablets were shown in Figure 5.

STABILITY STUDY OF TREPROSTINIL DIOLAMINE FAST DISSOLVING TABLETS.

Table 15: Comparison of Various Parameters for Stability Study

Evaluation Parameter	Initial	1month	2month	3month
Hardness(kg/cm ²)	3.1 ± 0.17	$3.2 \pm 0.36 = 7$	3.3 ± 0.04	3.3 ± 0.92
% Friability	0.26	0.25	0.23	0.23
Disintegration Time(sec)	5	7sec	8sec	9 sec
Drug Content	98.3	99.5	99.3	99.70

The optimized formulation TF3 is kept for stability studies. Accelerated stability studies were carried out at 40^{0} C / 75% RH for 3 months. The tablets were then evaluated for hardness, friability, disintegration and drug content at 1^{st} month, 2^{nd} month and 3^{rd} month. The results indicated that there was no significant change in evaluation of the tablets. The results were tabulated in Table 15.

Table 16: Comparison of Drug Release Profile of Batch TF3

Time(min)	Initial	1month	2month	3 month
2	65.4	64.92	63.54	62.43
4	74.8	73.70	72.24	71.65
6	82.65	81.08	80.03	79.65
9	89.05	88.92	87.24	86.08
10	96.97	95.98	94.83	94.02

The optimized formulation TF3 is evaluated for in-vitro drug release studies after keeping the table that accelerated stability conditions (40°C/75% RH) for 3months. It is evaluated initially, 1st month, 2nd month and 3rd month. In-vitro drug release studies were performed in phosphate buffer pH 6.8 by using USP dissolution test apparatus-Type II, Rotating Paddle method. The results indicated that there was no significant change in in-vitro drug release studies. The data for in-vitro release profile was shown in Table 16.

CONCLUSION

Rapimelt Tablets of The optimized can be successfully prepared by direct compression method using selected superdisintegrants with Crosspovidone 1.5%, 3%, 6%, Crosscarmellose 1.5%, 3%, 6% and Sodium starch glycolate 1.5%, 3%, 6%, for the better patient compliance and effective therapy the relative efficiency of these superdisintegrant to improve the disintegration and dissolution rate of tablets were found in order.

The disintegration of TF1, TF2, TF3 with 1.5%, 3%, 6% Crosspovidone formulations to be as 8, 6, 5secs respectively and is almost better than TF4, TF5, TF6, TF7, TF8, TF9 formulations. Formulation TF3 In-vitro Dissolution studie 10 minutes almost total amount of the drug is released 6% crosspovidone (i.e. 96.96%). Crosspovidone shows good result as compare to other superdisintegrants.

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